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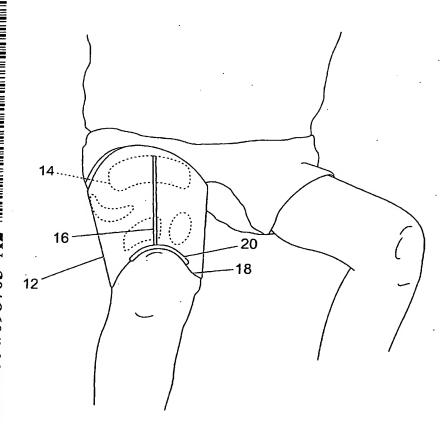
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(54) Title: APPARATUS FOR APPLYING ELECTRICAL CURRENT TO THE NEUROMUSCULAR SYSTEM



(57) Abstract: The invention relates to apparatus for applying electrical current to the quadriceps muscle. The apparatus is in the form of a garment (to be worn on a user's thigh) having a integrated programmable stimulation device including integral electronics. LCD display, user controls and a battery. To ensure accurate and repeatable positioning of the garment, it is shaped such that it locates above the patella. Furthermore, reference lines are provided on the skin facing surface of the garment to assist the user in the accurate placement of skin engaging electrodes. In combination, the features of the invention provides a safe and convenient means of electrically stimulating the quadriceps muscle irrespective of patient size whilst minimising the opportunity for Moreover, the invention dispenses with the need to employ a skilled clinician to individually place each electrode.

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1	Apparatus for Applying Electrical Current to the
2	Neuromuscular System
3	
4	The present invention relates to apparatus for
5	applying electrical current to muscles,
6	particularly, but not exclusively, to the quadriceps
7	muscle.
8	
9	Electrical stimulation of the quadriceps muscle is
10	well known. The quadriceps is the most important
11 .	muscle to be rehabilitated after an operation on the
12	knee. It is the strongest extensor of the knee and
13	improving the force of its contraction after surgery
14	consequently aids rehabilitation of the other
15	muscles involved in ambulation.
16	
17	The vastus medialis component of the quadriceps
18	stabilises the patella in the early stages of
19	walking. After knee surgery, not only can there be
20	a reflex inhibition of this muscle but there can
21	also be a temporary disruption of the joint receptor
22	activity which interferes with the patients

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Therefore the quadriceps 1 proprioceptive feedback. 2 muscle needs additional assistance in overcoming 3 this inhibition and early rehabilitation to aid 4 stability. 5 6 Although the quadriceps is a large muscle in the 7 front of the thigh, the knowledge of a clinical professional is required in order to accurately 8 position appropriately sized electrodes according to 9 patient size to thus ensure effective electrical 10 11 stimulation. The professional must ensure that the correct channels from a stimulator unit are 12 connected to correct electrodes on the right or left 13 14 leg. Whilst previous attempts to produce a failsafe garment for electrode application to the body 15 have succeeded in providing more convenient methods 16 17 of electrode application compared to traditional lead-wired systems, the assistance of a professional 18 has still been required in the initial set-up stage. 19 20 A further problem exists in terms of repeatability 21 in user application of the garment. This is often 22 inadequate since slight shifts in the position of 23 the electrode placement from day to day can change 24 the effectiveness of the stimulation, especially if 25 the garment is placed over a moving joint. 26 27 Many muscle groups have a symmetrical group on the 28 other side of the body across the coronal plane. 29 These muscle groups are mirror images of each other 30 and so the electrode placement should take account 31 of this. This has been achieved in certain garment 32

1	designs before by producing a mirror image garment
2	or by turning the existing garment inside out.
3	Where a stimulator unit and wiring is integrated in
4	the garment such a solution is not practical since
5	it would require the user to change the necessary
6	connections between the stimulator and the
7	electrodes thus introducing the opportunity for
8	error.
9	
10	According to a first aspect of the present invention
11	there is provided apparatus for applying an
12	electrical current to a neuromuscular system
13	comprising a garment adapted to cover a portion of a
14	user's body, a stimulation device for generating a
15	stimulating current connectable to at least one
16	electrical contact on said garment, the garment
17	being shaped to correspond with a particular
18	anatomical feature to ensure accurate and repeatable
19	positioning of the garment with respect to the
20	particular neuromuscular area to be treated.
21	
22	According to a second aspect of the present
23	invention there is provided apparatus for receiving
24	an electrical signal from a neuromuscular system
25 ·	comprising a garment adapted to cover a portion of a
26	user's body, a receiving device connected to at
27	least one electrical contact on said garment, the
28	garment being shaped to correspond with a particular
29	anatomical feature to ensure accurate and repeatable
30	positioning of the garment with respect to the
31	particular neuromuscular area to be monitored.
32	

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Preferably, the garment is marked with one or more 1 reference lines to aid the accurate and repeatable 2 positioning of the garment with respect to a 3 particular neuromuscular area. 5 6 Preferably, the neuromuscular area is the quadriceps muscle and the anatomical feature is the patella. 7 Preferably, the stimulation device is adapted such 9 10 that it is interactable with the garment to 11 100 determine whether it is a left-limb or right-limb 12 garment. 13 14 Preferably, the garment has an arcuate shaped edge at its distal end to correspond with the top of the 15 16 patella. 17 Preferably, the reference line is alignable with a 18 notional line extending upwardly from the centre of 19 20 the patella. 21 22 Preferably, the garment consists of an undergarment 23 and an over-garment, the undergarment having at 24 least one electrical contact on its skin-facing 25 surface conductively connected to one or more corresponding electrical contacts on its opposite 26 27 surface which, in turn, are conductively connected to contacts on the over-garment. 28 29 30 Preferably, the electrical connections between the undergarment and over-garment are made by stud 31

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fasteners which are fixed on and extend through the 1 2 undergarment. 3 Preferably, a plurality of electrical contacts are 4 provided on the undergarment. 5 6 7 Preferably, the or each electrical contact on the undergarment is conductively connectable to one or 8 more skin engaging electrodes. 9 10 Preferably, the or each skin engaging electrode is 11 user replaceable. 12 13 Preferably, four skin engaging electrodes are 14 15 employed. 16 Preferably, at least one skin engaging electrode has 17 a different surface area from the other skin 18 engaging electrodes. 19 20 Preferably, the combined surface area of the 21 electrodes is at least 300 cm<sup>2</sup>. 22 23 24 Preferably, the electrode having the greatest surface area extends across the upper quadriceps. 25 26 Preferably, at least one of the remaining electrodes 27 covers at least part of the lower fibres of the 28

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vastus medialis.

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Preferably, at least one of the remaining electrodes 1 2 covers at least part of the lateral fibres of the 3 quadriceps. 4 5 Preferably, one of the skin engaging electrodes is 6 generally dog-leg shaped. 8 Preferably, at least one of the skin engaging 9 electrodes is generally rectangular in shape. 10 Preferably, printed outlines of the skin engaging 11 12 electrodes are provided on the skin-facing surface of the undergarment to aid accurate positioning of 13 the electrodes by the user. 14 15 Preferably, the skin engaging electrodes are 16 displaced circumferentially to establish current 17 pathways which transect the neuromuscular area. 18 19 Preferably, the stimulation device includes control 20 means for selectively directing a stimulating 21 current to one or more of the skin engaging 22 23 electrodes. 24 25 Preferably, the control means includes user 26 programmable software for controlling the duration 27 of the stimulating pulses and their sequencing between the skin engaging electrodes. Preferably, the control means includes user programmable software for selecting any subset or all of the skin engaging electrodes in the garment

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to form one electrical pole and any other subset or 1 all of the remaining skin engaging electrodes in the 2 garment as the opposite electrical pole. 3 4 Preferably, the control means includes user 5 programmable software which allows the user to map б 7 control buttons on the garment such that current 8 applied to the medial and lateral quadriceps muscles is controllable by medial and lateral control 9 buttons respectively. 10 11 12 Preferably, the or each contact on the over-garment 13 is conductively connected to the stimulation device of the first aspect. 14 15 Alternatively, the or each contact on the over-16 garment is conductively connected to the receiving 17 device of the second aspect. 18 19 20 Preferably, the garment is securable to a user's 21 body by hook and loop fasteners. 22 Preferably, the garment is configurable for use on 23 the left or right leg. 24 25 Preferably, the connections between the stimulation 26 27 device and the at least one electrical contact on said garment are preset and non-alterable by the 28 user. 29 30 Preferably, the connections between the stimulation 31 device and the at least one electrical contact on 32

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said garment are non-alterable by the user by virtue 1 of the fact that they are integrated within the 2 3 garment itself. 4 5 An embodiment of the present invention will now be 6 described, by way of example only, with reference to 7 the following drawings, wherein: 8 9 Fig. 1 shows apparatus for applying current to the 10 quadriceps (undergarment and over-garment); Fig. 2 shows the inner and outer surfaces of the 11 undergarment; 12 13 Fig. 3 shows the inner and outer surfaces of the over-garment; 14 Fig. 4 shows the positioning of replaceable 15 electrodes on the leg; 16 Fig. 5 shows the apparatus in use; and 17 Fig. 6 shows the electrode sequencing of the 18 19 apparatus. 20 Fig. 1 shows apparatus for applying an electrical 21 current to a neuromuscular system, said system being 22 the quadriceps muscle, comprising an undergarment 12 23 provided with reference lines 14 and 16 24 25 respectively. A distal end 18 of the undergarment is provided with an arcuate shaped portion 20. 26 27 The term neuromuscular is to be understood to 28 include muscles, muscle parts, muscle groups, nerves 29

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or a combination thereof.

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The apparatus therefore locates unambiguously with 1 an appropriate anatomical landmark. The anatomical 2 locating means and corresponding anatomical landmark 3 must be selected such that the variation in 4 displacement of electrode positions with respect to 5 the anatomical location means is minimised for 6 individuals of different size. This allows a common 7 design to be used by different individuals with 8 minimal adjustment. 9 10 Typically, a useful anatomical reference is provided 11 by a "bony" reference point on the body where the 12 muscle position with respect to such a reference 13 point is consistent between individuals. According 14 to the present invention, the muscle and bony 15 reference point is the quadriceps and the patella 16 respectively. The patella is a sesamoid bone of the 17 quadriceps muscle and so, by effectively being part 18 of this muscle, it has a direct relationship to its 19 Regardless of the size of the patient, 20 movement. the lower fibres of the quadriceps insert via the 21 quadriceps tendon and then into the patella. 22 lower lateral fibres insert just above and laterally 23 . with respect to the patella. The vastus medialis 24 inserts a little lower on the medial side. 25 26 Accordingly, when designing a garment (see Fig. 1) 27 to assist with quadriceps electrode placement it has 28 been found that the following combination ensures 29 correct location in two axes: (i) an anatomical 30 locating means comprising an arcuate shaped edge 20 31 corresponding to the upper portion of the patella; 32

10

and (ii) a reference line 16 through the mid point 1 of the patellar curve and along the midline of the 2 3 thigh. 4 It will be appreciated by those skilled in the art 5 6 that the fitting of undergarment 12 to the leg and positioning it with the aid of the reference line 16 7 and the arcuate shaped portion 20 can be performed 8 by the user without any professional assistance. 9 10 Fig. 2 shows both the inner (skin facing) surface 30 11 and outer surface 32 of an undergarment adapted for 12 use on the right leg. Reference lines 34 are 13 provided on the inner surface 30 corresponding to 14 the shapes of replaceable electrodes A, B, C and D 15 for contacting the skin (discussed further below 16 with reference to Fig. 4). Alternative reference 17 lines 36 are also provided on the inner surface 30. 18 The reference lines 34 are not intended to be 19 visible on the outer surface 32 but are shown in 20 Fig. 2 as dashed lines 34 for clarity. 21 22 Electrical contacts 38 are provided on the inner 23 surface 30 of the undergarment and are conductively 24 connected to corresponding electrical contacts 40 on 25 26 the outer surface 32. 27 Velcro® straps 42 (i.e. hook and loop fasteners) are 28 provided on either side of the undergarment and an 29 arcuate shaped portion 44 (corresponding to 30 reference numeral 20 in Fig. 1) is provided at its 31 lower end. 32

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1 In use, replaceable electrodes for contacting a 2 user's skin are positioned on the skin facing 3 surface of the undergarment with the aid of the 4 reference lines 34. For some users (i.e. because of 5 their size of other specific requirements) replaceable electrodes A and D are positioned to 7 correspond with the alternative reference lines 36. 8 9 The undergarment is then fitted to the user's leg by 10 wrapping and securing the Velcro® straps 42 around 11 the thigh and aligning the arcuate shaped portion 44 12 with the top of the patella. The electrical 13 contacts 38 on the inner surface 30 therefore make 14 electrical contact with the replaceable electrodes 15 which in turn contact the user's skin over the 16 quadriceps muscle. The replaceable electrodes 17 electrically connect to the contacts 38 by means of 18 mating contacts or a conductive adhesive layer. 19 20 The contacts 38 are electrically connected to 21 contacts 40 on the outer surface 32 of the 22 undergarment. The electrical contacts 38 and 40 23 preferably comprise conductive stud fasteners which 24 are fixed on and extend through the fabric of the 25 undergarment. The flat surface of the stud fastener 26 presents on the inner surface 30 whereas a male or 27 female part of the stud fastener presents on the 28 outer surface 32. 29 30 The reference lines 34 and 36 and the electrical 31 contacts 38 are positioned to correspond with 32

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anatomical features such that upon correct 1 application and alignment of the garment to the leg, 2 electrodes of appropriate size, shape, orientation 3 and electrical connection are positioned on the leg. 4 5 Fig. 3 shows both the inner surface 50 and outer 6 surface 52 of an over-garment which is worn over the 7 undergarment of Figs 1 and 2. The inner surface 50 8 is provided with stud fasteners 54 which are 9 electrically connected to a stimulation device 56. 10 Control means 58 for controlling the stimulation 11 12 device are provided on the outer surface 52 of the 13 over-garment. 14 In use, the over-garment is attached to the 15 undergarment via their respective stud fasteners 54 16 A conductive path is thereby formed between 17 and 40. the stimulation device 56 and the replaceable 18 19 electrodes on a user's skin. 20 21 The over-garment is a flexible fabric envelope containing the stimulator electronics and a battery. 22 The control means 58 comprises an integral Liquid 23 Crystal Display (LCD) and button control panel 24 located on the outer surface 52 of the over-garment. 25 The user controls include two up and down controls 26 for medial and lateral muscles. The stimulator 27 internally re-maps these controls depending on 28 29 whether it is operating on a left or right undergarment. For example, on a left undergarment, 30 the rightmost amplitude control sets the intensity 31 of the medial muscle, whereas on the right 32

13.

1	undergarment it is the leftmost amplitude control
2	which sets the intensity of the medial muscle. This
3	is particularly important when the sequencing of the
4	muscle activation is required to recruit medial
5	before lateral muscles.
6	
7	Fig. 4 shows four replaceable electrodes A, B, C and
8	D which are positionable within the undergarment
9	and, in use, contact the user's skin. This figure
10	illustrates where each electrode typically locates
11	on the right leg when the undergarment is applied in
12	accordance with the user instructions. Electrode A
13	covers the upper quadriceps area while electrodes B
14	and C together cover the lower quadriceps area.
15	Electrode C locates medially while B locates more
16	centrally and extends laterally. Electrode D has a
17	dog-leg shape and is positioned to recruit the more
18	lateral fibres of the quadriceps.
19	
20	Electrode A: This is a large electrode in the
21	shape of a rectangle measuring 20 cm x 10cm (with
22	rounded corners) positioned so as to extend across
23	the upper quadriceps as illustrated. The electrode
24	extends equidistant either side of the mid-thigh
25	location mark and its lower edge is displaced 20cm
26	from the midpoint of the patellar locating arcuate
27	portion described previously. An alternative
28	position for electrode A is also provided to
29	accommodate taller users which is 22cm from the
30	patellar mark. This electrode has a surface area of
31	approximately 196 cm <sup>2</sup> .

14

This electrode is in the shape of a 1 Electrode B: 2 rectangle measuring 10 cm x 7.5 cm (again with 3 rounded corners) positioned so as to extend across the lateral portion of the quadriceps muscle close . 4 5 to the patella. The major midline of this electrode 6 is 7 cm from the patellar mark while the minor 7 midline is displaced 4 cm laterally from the midline 8 locating mark on the garment. This electrode has a 9 surface area of approximately 74 cm<sup>2</sup>. 10 11 Electrode C: This electrode is in the shape of a rectangle measuring 14cm x 6.5 cm (again with 12 rounded corners) which extends along the medial 13 portion of the quadriceps muscle close to the 14 15 patella. The major mid line of the electrode is 16 displaced 6 cm from the midline locating mark on the 17 garment and the minor midline of the electrode is 18 displaced 7 cm from the patellar locating edge. This electrode has a surface area of approximately 19  $82 \text{ cm}^2$ . 20 21 Electrode D: This is a small electrode which 22 locates laterally on the upper leg. 23 24 preferably dog-leg in shape and can be used on 25 either the right or left leg. This electrode has a 26 surface area of approximately 57 cm<sup>2</sup>. An alternative, more lateral, position for the 27 28 electrode is provided on the garment to accommodate 29 thighs of larger girth. 30 31 In this non-limiting example, the total area of all 32 four electrodes is approximately 410 cm<sup>2</sup>. However,

15

it will be appreciated that dimensions of the 1 electrodes can be varied and are typically greater 2 than 300 cm<sup>2</sup>. The electrodes are as large as 3 possible to recruit the target muscle with the 4 minimum current density at the skin. It is clear 5 that most of the anterior surface of the thigh is 6 covered by one or other of the electrodes and this 7 is very different to the established practice which 8 favours much smaller electrodes which require more 9 accurate placement. Using these much larger surface 10 area electrodes has proved successful in recruiting 11 the maximum number of muscle fibres whilst 12 minimising current density at the skin. 13 14 The relative sizes and positions of electrodes when 15 in place on the body define the current pathways 16 which can be created. When electrodes are placed on 17 a planar body surface then the penetration of the 18 electric field is not as good as when electrodes are 19 placed on a curved surface. By choosing electrode 20 positions which establish current pathways which 21 transect the body structure then stimulation of 22 deeper tissue can be achieved. The thigh, in simple 23 terms, is a cylindrical formation with little 24 curvature along its length but high curvature around 25 its circumference. Accordingly, by positioning one 26 electrode displaced circumferentially from another 27 electrode located at the anterior thigh midline we 28 achieve deeper penetration. The appropriate 29 dimensioning of this displacement with respect to 30 relevant anatomical markers ensures that selected 31 nerves are stimulated. 32

1	
2	The preferred positioning of the replaceable
3	electrodes is as follows. One large electrode
4	covering the upper fibres of the quadriceps and the
5	femoral nerve and (its upper branches). Two lower
6	electrodes cover the distal quadriceps fibres. The
7	inner lower electrode is sized and shaped so that it
8	covers the lower fibres of the vastus medialis.
9	This gives us the option to zone in on this muscle
10	separately for part of the rehabilitation. The
11	fourth electrode is an outer lateral electrode and
12	lies on the extreme lateral fibres of the quadriceps
13	and its main function is to direct the impulses from
14	the combination of electrodes in a different
15	direction. This electrode is displaced
16	circumferentially from the anterior thigh midline
17	and when used in conjunction with some or all of the
18	other electrodes creates current paths with transect
19	the thigh thereby stimulating deeper tissue. This
20	allows rehabilitation of a greater variety of fibres
21	within the muscle.
22	
23	The large surface areas of these electrodes allow
24	for a more comfortable contraction, because the skin
25	current density is reduced. Furthermore, this
26	reduces the necessity for precise adjustment of
27	electrode positioning between individuals.
28	
29	Fig. 5 shows the apparatus in use whereby the user
30	can control the stimulation of the quadriceps
31	muscle.

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The apparatus comprises an over-garment having an 1 integrated stimulation device which includes 2 integrated electronics, an LCD display, user 3 controls and a battery. The integrated nature of 4 the electrical connections means that the user does 5 not have to make individual connections between the 6 stimulator terminal and each replaceable electrode. 7 Apart from removing the requirement to select 8 electrical connections, such a system can 9 automatically change between left leg and right leg 10 modes by transposing connections and the mapping of 11 user controls and display elements. 12 13 While the apparatus may work with a simple single or 14 dual channel stimulator, it is preferable that the 15 apparatus is connected to an advanced stimulator, as 16 more fully explained below. This allows the 17 selection of any subset of electrodes as one 18 electrical pole (i.e. as a cathode) and any other 19 subset as the other electrical pole (i.e. as an 20 anode) and therefore creates a choice of current 21 pathways through the thigh. 22 23 The success of traditional Electrical Muscle 24 Stimulation (EMS) systems depend on the relative 25 positions of the array electrodes on the body, and 26 the correct connection to signal sources in the 27 stimulator. Any errors could lead to a completely 28 different current path in the body from that 29 intended. For this reason these techniques are not 30 suitable for general use with traditional exposed 31 leadwire systems which are prone to human error. 32

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1	The present apparatus solves this problem by
2	providing an electrode locating means, and an
3	electrode connection means within an integrated
4.	tamperproof garment. The electrode selections and
5	the timing thereof are as follows.
6	
7	The preferred apparatus has an integrated two-
8	channel electronic muscle stimulation garment
9	operating with four replaceable skin electrodes.
10	Preferably, the stimulation signal takes the form of
11.	a modulated pulse train, utilising a symmetric
12	biphasic pulse with interphase interval, operating
13	under constant current control. Each stimulation
14	pulse may be divided into a number of time segments,
15	called timeslots, and different electrode selections
16	can be made under software control for each
17	timeslot.
18	·
	- cc . E this approach is to achieve
19	The general effect of this approach is to achieve
19 20	larger effective electrode areas by combining the
	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin
20	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current
20 21	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into
20 21 22	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into timeslots with different electrode selections is to
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20 21 22 23 24 25	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into timeslots with different electrode selections is to vary the phase charge seen by each electrode and
20 21 22 23 24 25 26	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into timeslots with different electrode selections is to vary the phase charge seen by each electrode and therefore the intensity of stimulation associated
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20 21 22 23 24 25 26 27 28 29	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into timeslots with different electrode selections is to vary the phase charge seen by each electrode and therefore the intensity of stimulation associated with each electrode.  Where electrodes are combined to form an anode or
20 21 22 23 24 25 26 27 28 29	larger effective electrode areas by combining the areas of individual electrodes. This reduces skin current density for a given stimulation current level. The effect of dividing the pulse into timeslots with different electrode selections is to vary the phase charge seen by each electrode and therefore the intensity of stimulation associated with each electrode.  Where electrodes are combined to form an anode or cathode, then the current density at the skin is

that channel 1 is operable by the left hand 1 2 amplitude controls when fitted on a right leq undergarment, and by the right hand amplitude 3 control when fitted on a left leg undergarment. In 4 this way, the medial part of the muscle is always 5 6 operable by the medial amplitude control, whereas 7 the lateral muscle group is always operable by the lateral amplitude control. 8 9 A further example of electrode sequencing together 10 with the current patterns at each electrode is 11 provided in the second table in Fig. 6 with the 12 corresponding current patterns for each electrode 13 shown underneath. 14 (The current patterns are not to scale in either time or current amplitude) 15 16 17 Various modifications and improvements may be made without departing from the scope of the present 18 invention. 19 20 21 For example, an alternative to the arcuate shaped 22 portion which corresponds with the shape of the 23 patella could be a donut shaped locator at the 24 distal end of the undergarment. However this 25 design, as with any thigh garment with a knee 26 splint, would tend to pull on the undergarment proximally when the knee joint flexes. 27 28 29 Two versions of the undergarment could be provided, 30 one for the right and one for the left leq. identical array of stud fasteners would be provided 31 32 on either type however a different subset of

25

1

2 5. Apparatus according to any preceding claim

3 wherein, the stimulation device is adapted such that

4 it is interactable with the garment to determine

5 whether it is a left-limb or right-limb garment.

6

7 6. Apparatus according to claim 4 or 5 wherein,

8 the garment has an arcuate shaped edge at its distal

9 end to correspond with the top of the patella.

10

11 7. Apparatus according to any of claims 4 to 6

wherein, the reference line is alignable with a

notional line extending upwardly from the centre of

14 the patella.

15

16 8. Apparatus according to any of claims 1 to 7

wherein, the garment consists of an undergarment and

18 an over-garment, the undergarment having at least

one electrical contact on its skin-facing surface

20 conductively connected to one or more corresponding

21 electrical contacts on its opposite surface which,

in turn, are conductively connected to contacts on

23 the over-garment.

24

25 9. Apparatus according to claim 8 wherein, the

26 electrical connections between the undergarment and

27 over-garment are made by stud fasteners which are

fixed on and extend through the undergarment.

29

30 10. Apparatus according to claim 8 or 9 wherein, a

31 plurality of electrical contacts are provided on the

32 undergarment.

22

contacts would be used for the left and right 1 2 versions. An undergarment would be factory configured for left or right use by electrically linking one stud fastener in one of two alternative 4 positions. This would allow the stimulator 5 electronics to detect which undergarment is 6 7 connected and thereby direct the appropriate signals to each element of the stud array. Alternatively, 8 9 unused stud fasteners could be insulated with an insulating cover. 10 11 While the preferred apparatus includes the over-12 13 garment having an integrated stimulator device, it could be adapted for use with various conventional 14 electrical stimulation units. A simple single or 15 16 dual channel stimulator device could be connected to 17 the appropriate electrodes using, for example, leadwires terminating in stud faster contacts. For 18 general quadriceps rehabilitation both channels. 19 would be used. 20 21 In the case where a clinician needs to zone in on 22 extra rehabilitation of the vastus medialis the 23 medial channel is used alone. When both channels 24 are used there is a default feature that brings in 25 the contraction of the vastus medialis before the 26 27 rest of the bulk of the quadriceps. This is 28 particularly useful for the person with an unstable 29 patella. If the patella is prone to dislocation it 30 will invariably be in the lateral direction. In this 31 embodiment the patella is pulled slightly inwards and then upwards, ensuring stability of the patella. 32

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1 While the electrode configuration described has 2 several advantages it is also possible to use 3 smaller electrodes of conventional round and/or 4 rectangular shape. Accurate location of such 5 electrodes can still be achieved by a suitable 6 garment which includes the anatomical reference 7 means described (i.e. the patellar location arcuate 8 portion). The apparatus may include at least one 9 electrode and may include an array of electrodes 10 which will all locate correctly if referenced to the 11 12 locating means. 13 Any form of electrical therapy or biological signal 14 detection could be applied to this garment such as 15 TENS, EMG etc. Indeed, a combined dual function 16 stimulation and receiving device could be 17 incorporated into the garment (i.e. a combination of 18 the first and second aspects of the invention). 19 20 Garments for other muscle groups in the body could 21 also be included provided there was a fixed 22 relationship between the locating surface anatomical 23 feature and the intended muscle, muscle group or 24 nerve to this group. Examples of this may include 25 the reliable location of the common peroneal nerve 26 just below the fibular head or the ulnar nerve 27 behind the medial condyle of the humerus. 28. also be a specific relationship between anatomical 29 features and the movements of a muscle whether it 30 displaces with movement or simply shortens in an 31 isometric contraction. 32

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1 CLAIMS

2

3 1. Apparatus for applying an electrical current to

24

- 4 a neuromuscular system comprising a garment adapted
- 5 to cover a portion of a user's body, a stimulation
- 6 device for generating a stimulating current.
- 7 connectable to at least one electrical contact on
- 8 said garment, the garment being shaped to correspond
- 9 with a particular anatomical feature to ensure
- 10 accurate and repeatable positioning of the garment
- 11 with respect to the particular neuromuscular area to
- 12 be treated.

13

- 14 2. Apparatus for receiving an electrical signal
- 15 from a neuromuscular system comprising a garment
- 16 adapted to cover a portion of a user's body, a
- 17 receiving device connected to at least one
- 18 electrical contact on said garment, the garment
- 19 being shaped to correspond with a particular
- anatomical feature to ensure accurate and repeatable
- 21 positioning of the garment with respect to the
- 22 particular neuromuscular area to be monitored.

23

- 24 3. Apparatus according to claim 1 or 2 wherein,
- 25 the garment is marked with one or more reference
- lines to aid the accurate and repeatable positioning
- of the garment with respect to a particular
- 28 neuromuscular area.

- 30 4. Apparatus according to any preceding claim
- 31 wherein, the neuromuscular area is the quadriceps
- 32 muscle and the anatomical feature is the patella.

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1

- 2 11. Apparatus according to any of claims 7 to 9.
- 3 wherein, the or each electrical contact on the
- 4 undergarment is conductively connectable to one or
- 5 more skin engaging electrodes.

6

- 7 12. Apparatus according to claim 11 wherein, the or
- 8 each skin engaging electrode is user replaceable.

9

- 10 13. Apparatus according to claim 11 or 12 wherein,
- four skin engaging electrodes are employed.

12

- 13 14. Apparatus according to claim 13 wherein, at
- least one skin engaging electrode has a different
- 15 surface area from the other skin engaging
- 16 electrodes.

17

- 18 15. Apparatus according to claim 13 or 14 wherein,
- 19 the combined surface area of the electrodes is at
- least  $300 \text{ cm}^2$ .

21

- 22 16. Apparatus according to claim 14 wherein, the
- 23 electrode having the greatest surface area extends
- 24 across the upper quadriceps.

25

- 26 17. Apparatus according to claim 16 wherein, at
- 27 least one of the remaining electrodes covers at
- least part of the lower fibres of the vastus
- 29 medialis.

- 1 18. Apparatus according to claim 16 wherein, at least one of the remaining electrodes covers at
- 3 least part of the lateral fibres of the quadriceps.

4

- 5 19. Apparatus according to any of claims 11 to 18
- 6 wherein, one of the skin engaging electrodes is
- 7 generally dog-leg shaped.

8

- 9 20. Apparatus according to any of claims 11 to 19
- wherein, at least one of the skin engaging
- 11 electrodes is generally rectangular in shape.

12

- 13 21. Apparatus according to any of claims 11 to 20
- wherein, printed outlines of the skin engaging
- electrodes are provided on the skin-facing surface
- of the undergarment to aid accurate positioning of
- 17 the electrodes by the user.

18

- 19 22. Apparatus according to any of claims 11 to 21
- 20 wherein, the skin engaging electrodes are displaced
- 21 circumferentially to establish current pathways
- 22 which transect the neuromuscular area.

23

- 24 23. Apparatus according to any of claims 11 to 22
- 25 wherein, the stimulation device includes control
- 26 means for selectively directing a stimulating
- 27 current to one or more of the skin engaging
- 28 electrodes.

- 30 24. Apparatus according to claim 23 wherein, the
- 31 control means includes user programmable software
- 32 for controlling the duration of the stimulating

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28

pulses and their sequencing between the skin 1 2 engaging electrodes. 3 Apparatus according to claim 23 or 24 wherein, 4 the control means includes user programmable 5 6 software for selecting any subset or all of the skin 7 engaging electrodes in the garment to form one electrical pole and any other subset or all of the 8 9 remaining skin engaging electrodes in the garment as 10 the opposite electrical pole. 11 Apparatus according to any of claims 23 to 25 12 wherein, the control means includes user 13 programmable software which allows the user to map 14 15 control buttons on the garment such that current applied to the medial and lateral quadriceps muscles 16 is controllable by medial and lateral control 17 18 buttons respectively. 19 27. Apparatus according any of claims 8 to 26 when 20 dependent on claim 1 wherein, the or each contact on 21 the over-garment is conductively connected to the 22 stimulation device. 23 24 Apparatus according to any of claims 8 to 27 25 26 when dependent on claim 2 wherein, the or each contact on the over-garment is conductively 27 connected to the receiving device. 28

29

30 Apparatus according to any preceding claim 31 wherein, the garment is securable to a user's body

32 by hook and loop fasteners. 1

- 2 30. Apparatus according to any preceding claim
- wherein, the garment is configurable for use on the
- 4 left or right leg.

5

- 6 31. Apparatus according to any preceding claim
- 7 wherein, the connections between the stimulation
- 8 device and the at least one electrical contact on
- 9 said garment are preset and non-alterable by the
- 10 user.

- 12 32. Apparatus according to claim 31 wherein, the
- connections between the stimulation device and the
- 14 at least one electrical contact on said garment are
- integrated within the garment itself.

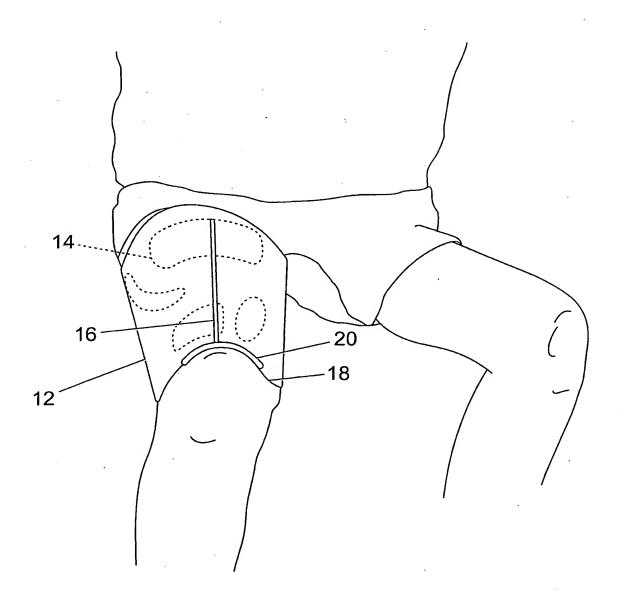


Fig. 1

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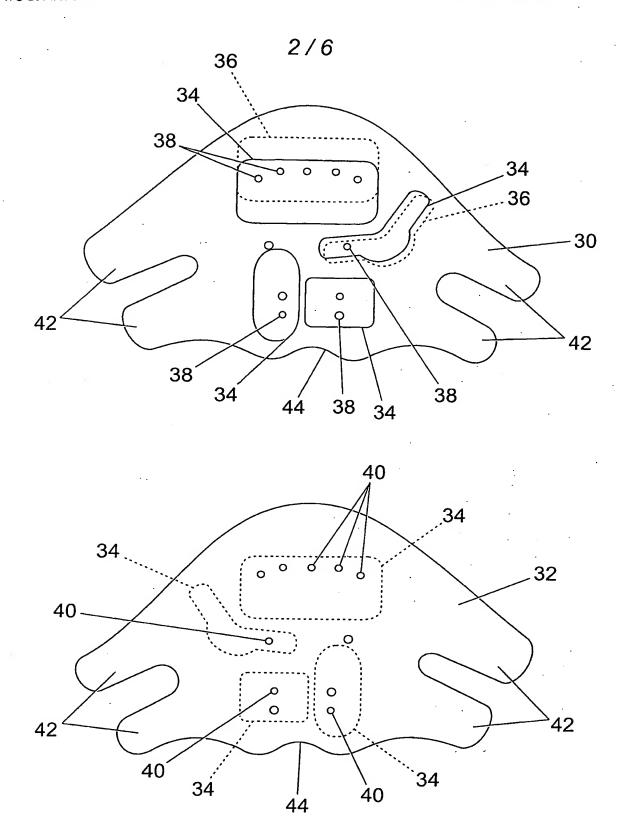
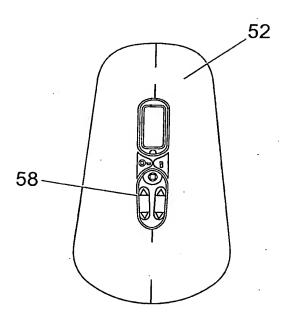


Fig. 2
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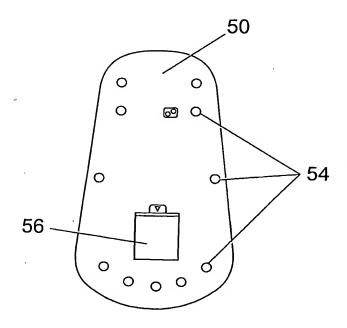
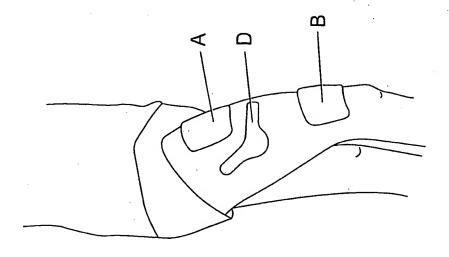


Fig. 3

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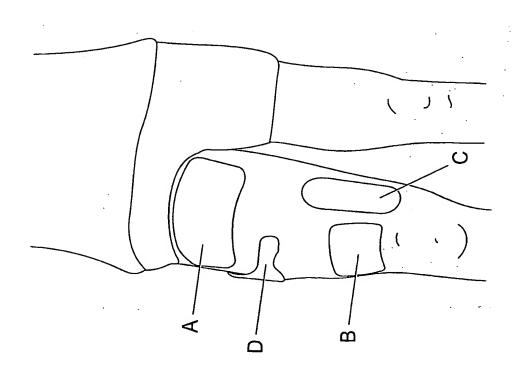


Fig.

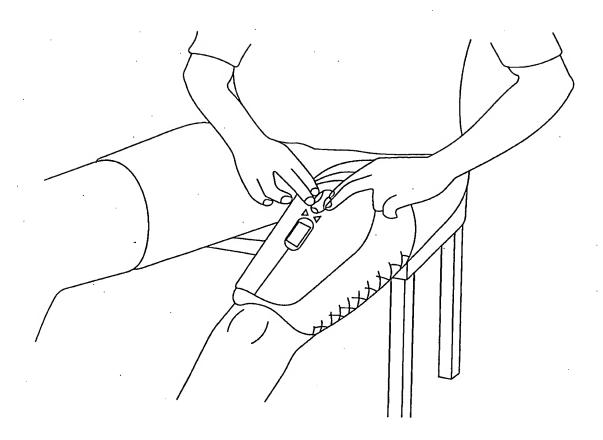


Fig. 5

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Pad	CH1 TS1	CH2 TS1	CH2 TS2
A	Н	<u>L</u>	<u> </u>
В	H	H	X
C	L	Н	X
Ď	H	X	H
Duration uS	100	300	100

CH1	Timeslot 1	Timeslot 2
A	Hi	Hi
В	Hi	Hi
C	Lo	Lo
D	Hi	H
Duration	100uS	100uS

CH2	Timeslot 1	Timeslot 2
Α	Lo	Lo
В	Hi	X
C	Hi	X
D :	X	Hi
Duration	600uS	200uS

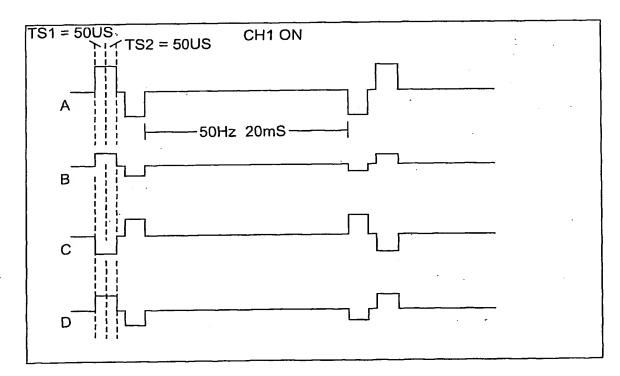


Fig. 6
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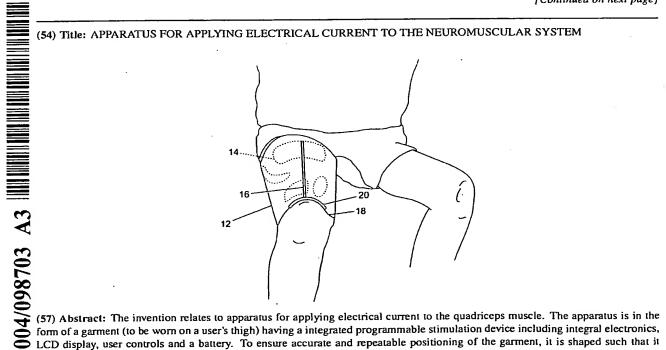
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[Continued on next page]



form of a garment (to be worn on a user's thigh) having a integrated programmable stimulation device including integral electronics, LCD display, user controls and a battery. To ensure accurate and repeatable positioning of the garment, it is shaped such that it locates above the patella. Furthermore, reference lines are provided on the skin facing surface of the garment to assist the user in the accurate placement of skin engaging electrodes. In combination, the features of the invention provides a safe and convenient means of electrically stimulating the quadriceps muscle irrespective of patient size whilst minimising the opportunity for error. Moreover, the invention dispenses with the need to employ a skilled clinician to individually place each electrode.

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 $\begin{array}{ll} \mbox{MinImum documentation searched} & \mbox{(classification system followed by classification symbols)} \\ \mbox{IPC} & 7 & \mbox{A61N} & \mbox{A61B} \\ \end{array}$ 

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the International search (name of data base and, where practical, search terms used)

EPO-Internal, PAJ, WPI Data

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	paragraphs '0034!, '0037!, '0041!	
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Date of the actual completion of the international search  11 November 2004	Date of mailing of the international search report  19/11/2004	
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